Claims 28 and 33 are independent claims based on cancelled claim 9 incorporating the composition of the wire which made claims 12 and 20 allowable. Therefore new claims 28 and 33 are believed to be allowable and claims new claims 29-32 and 34-37 are dependent on allowable claims 28 and 33 as believed to be allowable.

Since all claims now appear to be allowable the applicant prays that the claims be passed to allowance.

Respectfully submitted,

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VERSION WITH MARKINGS TO SHOW CHANGES MADE TO THE SPECIFICATION

On page 1, in the first paragraph of the Description of the Related Art please amend the paragraph as follows:

A major requirement for guidewires and other guiding members, whether they [be] are solid wire or tubular members, is that they have sufficient column strength to be pushed through [a] passageways in a patient such as the patient's vascular system with minimal kinking or binding. However, the distal section of the guidewire must be flexible enough to avoid damaging the blood vessel or other body lumen through which it is advanced. Efforts have been made to improve both the strength and flexibility of guidewires to make them more suitable for their intended uses, but strength for pushing and flexibility for turning without damaging vascular walls tend to be diametrically opposed to one another, in that an increase in one usually involves a decrease in the other. There has been a gradual decrease in the profiles or transverse dimensions of commercially available intravascular catheters and guidewires particularly for use in coronary arteries. However, concomitant with the decrease in profile has been a loss in pushability and kink resistance.

On page 2 fourth full paragraph please amend the paragraph as follows:

NiTi guidewires tend to be too springy, especially when negotiating a tortuous path in vessels, they do not have good pushability because want to straighten out or return to their original shape. NiTi guidewires will readily get hung up when rotated while extending around a curved path. NiTi guidewires can not be torqued as readily as stainless steel because it is

[more springy] springier. NiTi guidewires tend to have good shape memory. The shape memory makes it difficult for a physician[.] to shape the tip of the guidewire with his fingers for accessing difficult to reach portions of the patient's vascular system.

On page 6 in the 2nd paragraph please amend the paragraph as follows:

A guidewire is shown in Fig. 1 having a titanium molybdenum alloy which [is] has properties between that of stainless steel and NiTi alloys. The titanium molybdenum alloy is easier to use and has better [rotatability] torque, softness and pushability for use in the passageways of patients than guidewires made of other materials.

On page 7 in the first paragraph please amend the paragraph as follows:

Alternatively the guidewires can be made with a range of values for its alloys. The range of values is approximately 75-83% titanium, 8-14% molybdenum, 4-8% zirconium and 2-6% tin by weight.

On page 7 in the fourth paragraph please amend the paragraph as follows:

A guidewire made from a titanium molybdenum alloy is less springy than NiTi alloys [and] but more springy than stainless steel. Titanium molybdenum alloys are stiffer than NiTi alloys [and] but not as stiff as stainless steel. Therefore titanium molybdenum alloys have desirable properties when used in guidewires.

On page 7 the last paragraph bridging onto the next page please amend the paragraph as follows:

Figure 2 shows the relative stress and strain curves comparing NiTi alloys, curve 35, stainless steel, curve 30 and titanium molybdenum alloy, curve 33 guidewires. The graph charts the percentage of maximum bending moment (inch=pounds) as related to the angular deflection (degrees). It shows the percentage that each wire returns to [it's] its original shape after being bent to a given moment. As shown on the chart, when deflected, Nitinol returns to [it's] its shape, stainless steel returns to only about 5% of it's original shape and titanium molybdenum alloy such as Beta III alloy returns to about 50% of its original shape. Thus the titanium molybdenum alloy such as Beta III alloy exhibits springback properties between Nitinol and Stainless [staeel] steel.

On page 8 the first full paragraph please amend the paragraph as follows:

Fig. 1 shows a side view of a guidewire 10 having a proximal end 12 and a distal end 14. The distal end 14 has a smaller diameter than the proximal end 12 to make [is] it softer and more easily bendable. It is desirable to have a softer distal end 14 such that the guidewire will bend and follow the curves of a blood vessel or other passageway that the guidewire is inserted into. The guidewire is provided with a rounded distal tip 16 at the tip of the distal end 15 to secure the coil 18 to the distal end 14 and to prevent the tip of the distal end 15 from [poking thought] penetrating tissue in the passageway as the guidewire is being inserted. The guidewire 10 is also provided with a coil 18 which can be made out of platinum, tungsten or similar radioopaque materials to act as a spring, allowing the thinned distal end 14 to bend

and yet spring back into place after the guidewire is transported around a curve in the passageway.

On page 9 second full paragraph please amend the paragraph as follows:

Abrupt changes in the stiffness of the distal end of the guidewire causes kinking at stress points of the coil, when the distal end is bent. By having a larger number of tapered sections with small changes in the diameter the flexibility (bendability) of the guidewire can continually increase toward the distal end of the guidewire 14 without an abrupt change averting kinking.

On page 9 fourth full paragraph please amend the paragraph as follows:

The titanium molybdenum alloy steers better than stainless steel guidewires or NiTi alloy guidewires because it is more flexible than stainless steel yet stiff enough to have torque and [it] is stiffer than NiTi.

On page 10 third paragraph please amend the paragraph as follows:

The guidewire 10 can be made with lengths of preferably between 20 cm and 500cm and between diameters of 0.005 inches and 0.040 inches with a coil length preferably of between 0.5cm and 100cm.[...]